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A universal self-charging system driven by random biomechanical energy for sustainable operation of mobile electronics

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Human biomechanical energy is characterized by fluctuating amplitudes and variable low frequency, and an effective utilization of such energy cannot be achieved by classical energy-harvesting technologies. Here we report a high-efficient self-charging power system for sustainable operation of mobile electronics exploiting exclusively human biomechanical energy, which consists of a high-output triboelectric nanogenerator, a power management circuit to convert the random a.c. energy to d.c. electricity at 60% efficiency, and an energy storage device. With palm tapping as the only energy source, this power unit provides a continuous d.c. electricity of 1.044 mW (7.34 Wm^{-3}) in a regulated and managed manner. This self-charging unit can be universally applied as a standard 'infinite-lifetime' power source for continuously driving numerous conventional electronics, such as thermometers, electrocardiograph system, pedometers, wearable watches, scientific calculators and wireless radio-frequency communication systems and internet of things.

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rapid development in personal electronics and sensor networks^{1,2} has raised urgent and challenging requirements for their portable and sustainable power sources, which are now mostly using batteries. In many modern mobile electronics and internet of things, batteries have become the largest and heaviest component of the entire unit, and they are required to be charged periodically due to limited lifetime, leading to an inevitable design trade-off dilemma between mobility (size and weight) and sustainability (lifetime). Although this dilemma can be eased to some extent with the development of high-energy-density materials³⁻⁵, it is not solved from the root. A fundamental solution to this challenge is to develop technologies that can constantly convert ambient energy into electricity and get the battery continuously charged to ensure its sustainable and maintenance-free operation⁶⁻⁸. Ambient energy sources exist in various forms, such as mechanical, thermal^{9,10}, chemical¹¹ and solar^{12,13}. Distinguished from others, mechanical energy is the one that is available almost everywhere and at any time, to name a few, gentle airflow, ambient sound, vibration, human body motion, ocean waves and so on. Although this type of energy could be converted by using traditional generators based on electromagnetic induction, they are usually heavy in weight and large in size. More importantly, their designs are rigid and cannot be easily adapted for harvesting body motion energy and vibration energy due to their intrinsic structure complexity^{14–17}. Finally, as limited by the working mechanism, an electromagnetic generator usually produces a small output voltage (<1 V) when its size is small, so that the output power cannot be effectively utilized because of the threshold voltage required to overcome a diode to function in rectification. Alternatively, micro-electromechanical-based energy harvesting using electrostatic or piezoelectric effect commonly provides a power level of $\sim \mu W$ (refs 18–23), so it can hardly meet the needs for wearable and portable electronics that require mW-W level of power.

Contact electrification, known for thousands of years, is about charge transfer between two materials when they contact with each other, but this effect is rarely utilized for energy harvesting until recently^{24,25}. Triboelectric nanogenerators (TENGs) were invented by incorporating contact electrification and electrostatic induction, and it has been demonstrated as a promising technology with numerous advantages, including large power density, high efficiency, diverse choice of materials for fabrication, low cost and lightweight²⁶⁻²⁹. TENG has various working modes that cover almost all of the mechanical motions in our daily life. Besides, it can be made into thin-film structure with high compactness and three-dimensional integration scalability that can potentially lead to mW-W output power. However, to embed TENGs into electronic system for practical applications, there are major challenges to overcome. First, due to the randomness of mechanical energy source and the intrinsic capacitive behaviour of TENGs, the output of a TENG normally is in the form of pulsed a.c. signal with variable frequency³⁰. Second, TENG usually has a high output voltage in the order of hundreds of volts but low current in the order of microamps, which has a huge mismatch with the requirement of mobile electronics. Besides, the high inherent impedance of TENGs results in ultralow energy conversion efficiency using conventional transformer for power management. Third, owing to the a.c. output, TENGs cannot be taken as steady power sources for directly driving electronics. Therefore, an energy storage unit is necessary to serve as a 'reservoir' for collecting the generated charges and outputting them in a managed and regulated manner. However, a direct integration of a TENG with an energy storage device has shown extremely low charging efficiency and large power loss due to the huge impedance mismatch between TENGs and energy storage

units, where TENGs have inherently high impedance while energy storage devices such as batteries and capacitors usually have low impedance^{31,32}. Therefore, although there are several TENG-based 'self-powered' systems being reported, all of these systems either cannot work continuously due to the low level of generated d.c. power or the entire system cannot be exclusively driven by the harvested energy if the data measurement and processing systems as well as data transmission components are included.

Here we present a genuine self-powered system to meet mW requirement of personal electronics by solving the challenges presented above. The system includes a TENG, a power management circuit and a low-leakage energy storage device. We perform system-level optimization to ensure the collaborative work of all the system components. Especially, a power management circuit is designed to solve the impedance mismatch problem, which can achieve 90% board efficiency and 60% total efficiency, about two orders of magnitude improvement compared with direct charging. Driven by palm tapping, this power unit can provide a continuous d.c. electricity of 1.044 mW on average power in a regulated and managed manner that can be universally applied as a standard power source for continuously driving numerous conventional electronics, such as a thermometer, a heart rate monitor (electrocardiograph (ECG) system), a pedometer, a wearable electronic watch, a scientific calculator and a wireless radio-frequency communication system. Our study demonstrates the first power unit that utilizes widely accessible biomechanical energy source to sustainably drive a broad range of commercial mobile and wearable electronic devices.

Results

Design of the system framework. This integrated humanmotion-driven self-powered system is shown in Fig. 1, including a human-motion-powered self-charging power unit and functional circuits for different applications. The TENG scavenges the human biomechanical energy and converts it to a.c. electricity. Then this a.c. electricity is converted to a d.c. electric output that matches to the input of the energy storage unit by the power management circuit. Finally, the energy storage unit provides d.c. electricity to the whole functional circuits, including sensors, data processors, displays and wireless transmitters. The signals from sensors and data processors are either visualized on a LCD displayer or sent out remotely through a wireless transmitter.

Design of the multilayered TENG. The TENG is first designed and optimized to efficiently harvest human biomechanical energy. We choose a multilayered attached-electrode contact-mode TENG to effectively collect the energy from human walking and running. The basic working principle of attached-electrode contact-mode TENGs is shown in Fig. 1b, which utilizes the conjugation between contact electrification and electrostatic induction³³. As shown in Fig. 1c, a Kapton film is shaped into a zigzag structure with 10-15 layers³⁴. For each layer, a thin aluminium foil and fluorinated ethylene propylene (FEP) layer are utilized as the triboelectric materials. The Al foil also serves as one electrode. Copper is evaporated at the backside of the FEP layer as the other electrode. As shown in Fig. 1d, the as-fabricated TENG has small volume and lightweight $(5.7 \times 5.2 \times$ 1.6 cm/29.9 g for a 10-layer TENG and $5.7 \times 5.2 \times 2.4$ cm/43.6 g for a 15-layer TENG). The optimum thickness of FEP for this design is 125 µm according to theoretical calculation and structural design considerations (Supplementary Fig. 1). Besides, nanostructures are created on the surface of FEP and Al foil to enhance the device performance (Supplementary Fig. 2) 35 . Embedded in the shoe insoles, a human walking can drive this



Figure 1 | Structure design of the self-powered system. (a) System diagram of a TENG-based self-powered system. (b) Working mechanism of an attached-electrode contact-mode TENG. (c) Structure of the designed multilayer TENG. (d) Photo of an as-fabricated TENG. (e) Short-circuit current output and (f) open-circuit voltage output of the as-fabricated TENG.

TENG to generate about $2.2 \,\mu\text{C}$ short-circuit transferred charge and about 700 V voltage output, as shown in Fig. 1e,f. This multilayered TENG is able to work reliably in various kinds of environment. Distinguished from the sliding TENGs, this contact-separation working mechanism ensures little friction and abrasion of the two surfaces during the contact and separation processes, which hugely enhance the durability of this device. As shown in the durability test (Supplementary Fig. 20), the normalized transferred charge does not show obvious degradation even after about 180,000 cycles. Besides, humidity and moisture has also been proven to have little effect to the TENG's performance in a previous study³⁶.

Design of the power management circuit. The key technical challenge is to efficiently store the TENG a.c. electric energy into an energy storage unit. Traditionally, a bridge rectifier is used to convert the a.c. to d.c. and then the energy is directly stored into a large capacitor or a battery (called direct charging)³². However, since TENGs have inherently high impedance, such design always faces a huge impedance mismatch especially when the energy source is low-frequency human biomechanical energy, resulting in ultralow energy storage efficiency³¹. For example, if a TENG is used to directly charge an ideal 1-V battery, the theoretical total efficiency η_{total} is only about 1% even when the battery's current leakage and internal resistance are neglected (Supplementary Discussion, Section 3.3). Another possible method is to utilize a transformer to match the impedance between the TENG and the energy storage device. However, since TENGs have high internal impedance and pulsed signal output, all practical transformers suffer a huge loss in power conversion,

as dictated by their limited quality factor, insufficient primary inductance, poor low-frequency response and finite narrow bandwidth.

Therefore, a new design is required to solve this challenge. From our previous work, when a TENG is utilized to charge a capacitor C_{temp} through a bridge rectifier under periodic mechanical motion (initial voltage of C_{temp} is 0 V), the voltage of C_{temp} (V_{temp}) has the following relationship with the charging time *t* (ref. 31):

$$V_{\text{temp}} = V_{\text{sat}} \left[1 - \exp\left(-\frac{kft}{C_{\text{temp}}} \right) \right]$$
(1)

where V_{sat} and k are parameters determined by the TENG's design, and f is the external mechanical motion frequency. Accordingly, the average power (P_{avg}) stored in C_{temp} from time 0 to t can be given by:

$$P_{\text{avg}} = \frac{C_{\text{temp}} V_{\text{temp}}^2}{2t} = \frac{C_{\text{temp}} V_{\text{sat}}^2}{2t} \left[1 - \exp\left(-\frac{kft}{C_{\text{temp}}}\right) \right]^2$$
$$= P_0 \frac{\left[1 - \exp(-x)\right]^2}{x}$$
(2)

where a dimensionless parameter *x* is defined as kft/C_{temp} and P_0 is a power constant defined as $kfV_{\text{sat}}^2/2$. As shown in Fig. 2b, there is an optimized x_{opt} equal to 1.25643

As shown in Fig. 2b, there is an optimized x_{opt} equal to 1.25643 when the P_{avg} reaches its maximum value of 0.4073 P_0 . At this optimized x_{opt} (t_{opt}), V_{temp} reaches 0.7153 V_{sat} , which is the optimized charging voltage V_{opt} . Note that V_{opt} only depends on TENG parameters (independent of C_{temp}). At this point, η_{total} reaches 75.0%, which is the highest charging efficiency for a



Figure 2 | Design of the power management part for regulated TENG outputs. (a) Circuit diagram of the power management circuit. (b) Theoretical calculation of the optimized charging time to demonstrate the design of the power management circuit. (c) Board efficiency measurement results. (d) Measurement of the maximum d.c. power of this system driven by human biomechanical energy. (e,f) Total efficiency measurement results. (e) Measurement of the a.c.-harvested power from a resistor. (f) Measurement of the d.c.-harvested power from the power management circuit. (g) Comparison of the charging current between direct charging and board charging.

capacitor charged from 0 V by TENG (Supplementary Discussion, Section 3.4).

With the above theoretical understanding of TENG charging characteristics, we can design the following charging strategy for maximized energy storage efficiency. First, a small temporary capacitor (C_{temp}) is charged by the TENG from 0 V. Once its voltage reaches V_{opt} (impedance match condition is reached), the energy stored in C_{temp} begins to be transferred to the final energy storage unit (a large capacitor or a battery) to maximize η_{total} . When the energy transfer finishes, the voltage of C_{temp} drops back to close to 0, and then C_{temp} is recharged by the TENG to reach V_{opt} again. With this optimized charging cycle, η_{total} can theoretically reach 75% (Supplementary Discussion, Section 3.4).

This theoretical charging cycle can be realized by a two-stage power management circuit, as shown in Fig. 2a. At the first stage, a temporary capacitor C_{temp} is charged by a TENG through a bridge rectifier. The second stage is for energy transfer from C_{temp} to the final energy storage unit. Since transferring electrostatic energy directly from a small capacitor to a large capacitor (or a battery) results in huge energy loss (Supplementary Discussion, Section 4), two automatic electronic switches (controlled by a logic control unit, the power of both switches and their logic control unit is supplied from the final energy storage unit) and a coupled inductor are utilized in the second stage^{37,38}. The detailed operation process is shown below to achieve efficient energy transfer in this stage. First, both the switches J_1 and J_2 are open to avoid interference of the charging process of C_{temp} . When V_{temp} reaches V_{opt} electronic switch J_1 closes. As a result, the energy starts to transfer from C_{temp} to inductor L_1 and V_{temp} starts to drop. When the energy is thoroughly transferred to L_1 , the switch J_1 opens and J_2 closes. As a consequence, the current of L_1 falls to 0 instantaneously. Besides, since the total magnetic flux linkage in the coupled inductance cannot change abruptly, the current of L_2 will suddenly rise up, corresponding to the energy transfer from L_1 to L_2 . Finally, the energy stored in L_2 will automatically transfer to the final energy storage unit because of the closure of J_2 . When the energy stored in L_2 is thoroughly sent out, J_2 is open again and another charging cycle begins.

Performance of the power management circuit. The operation of such a power management system is shown in Fig. 2c–g. Figure 2c shows the voltage profiles of both temporary capacitor (V_{temp}) and final storage capacitor (V_{store}) when one 15-layer TENG and a 1-mF Al-electrolyte capacitor were utilized as the energy harvester and the energy storage unit (C_{store}) , respectively (Supplementary Fig. 9). While the TENG is driven by palm tapping, C_{temp} is charged by the TENG and discharged through the energy transfer network, resulting in an oscillation of V_{temp} between 230 and 0 V. During the drop phase of V_{temp} . Note that if there was no mechanical energy input (from 5.4 to 5.7 s in Fig. 2c), both V_{temp} and V_{store} will decrease slowly because of the system leakage current and the power consumption of the electronic switches. The performance of the energy transfer network can be evaluated by the board efficiency (η_{board}), which is defined as the ratio of the

total energy stored in C_{store} to the total energy transferred out from C_{temp} . From the data shown in Fig. 2c, the total energy sent out from C_{temp} is calculated as 9.160 mJ, while the total energy stored in C_{store} is calculated as 8.243 mJ (Supplementary Discussion, Section 5). So this energy transfer network has $\eta_{\text{board}} = 90.0\%$, which is hugely improved in comparison with that of one-step direct energy transfer process (Supplementary Discussion, Section 4).

To measure the d.c. power delivered to the load by the system as driven by palm tapping, a load resistor R_L is connected in parallel with the storage capacitor (see Supplementary Discussion Section 3.2 for detailed experimental configuration). The storage capacitor C_{store} is charged by two 15-layer as-fabricated TENGs and then provides d.c. power for R_L. As shown in Fig. 2d, when $R_{\rm L}$ is high, the power consumption of $R_{\rm L}$ is lower than the power provided by TENG, so V_{store} has a positive slope with time. As the load resistance $R_{\rm L}$ decreases, the load power consumption increases and the charging slope of V_{store} decreases. When the charging slope reduces to 0 (39 k Ω , Supplementary Fig. 5), the power delivered from palm tapping is the same as the power consumed on the load, which is calculated as 1.044 mW (7.34 W m^{-3}) . When R_{L} continues to decrease $(20 \text{ k}\Omega)$, the power delivered from palm tapping is not enough to compensate the energy consumption on the load, and the charging slope becomes negative.

The most important parameter of the power management circuit is the total efficiency η_{total} , which is defined as the ratio of the maximum d.c. power stored into the storage unit to the maximum a.c. power delivered to a resistive load (Supplementary Discussion, Section 3). To measure η_{total} , first the maximum a.c. power delivered to a resistive load can be extracted by the TENG resistance-matching measurement (Supplementary Fig. 8). As shown in Fig. 2e, the maximum a.c. energy generated by TENG is 0.3384 mW at an optimum load resistance of 4.26 M\Omega. Second, the maximum d.c. power delivered through the power management board can be measured using the method shown above, which is 0.2023 mW (Fig. 2f) under the same mechanical triggering (from an electric motor). Therefore, η_{total} is calculated as 59.8%.

Compared with direct charging, the power management board shows a huge enhancement of the charging efficiency. In another supercapacitor charging experiment (see Supplementary Discussion Section 6 for detailed experimental configuration), the net supercapacitor charging current is 13.82 nA through direct charging and 15.14 μ A through the designed power management board, which is improved by as high as 1,096 times! Note that a transformer shows even worse performance than direct charging. As shown in Supplementary Fig. 11, the charging current of a supercapacitor cannot even compensate the leakage current when a 10:1 transformer is utilized as the impedance match network.

Broad applications as a sustainable d.c. power source. This human-motion-charged power unit have wide applications in realizing self-powered human-activity sensors, which makes them self-sufficient without any external power sources. Several applications have been demonstrated by utilizing this self-charged unit to sustainably drive various commercial electronic systems (Fig. 3a). In the first demo, this human-motion-charged power unit was connected to a commercial temperature sensor (Fig. 3b, detailed system diagram is shown in Supplementary Fig. 12). This temperature sensor utilizes a thermal couple to sense the external environment temperature. Then the sensing analogue signal is digitalized through an analogue–digital converter (ADC). Finally, the digital signal is shown on a LCD display to fulfil the

visualization of the output. As shown in Supplementary Movie 1, even under very gentle 1.6 Hz palm tapping (palm tapping is utilized mainly for easier filming purpose, other kinds of human motion such as foot tapping is also suitable for the application), this human-motion-charged power unit could supply enough power to maintain continuous operation of the temperature sensor. There were not any external power sources/batteries inside to power any part of the whole functionalized system.

This kind of power unit can also serve as power source for human health monitoring. As a typical example, we realized a self-powered ECG system (Fig. 3c, detailed system diagram shown in Supplementary Fig. 13). The bioelectricity signal across human left hand and right hand was first collected through the ECG signal collector (two conducting Al rods), and then amplified and filtered through an ECG signal amplifier (AD8232, Analog Devices). Such amplified heart rate signal was shown in Supplementary Fig. 14. After that, an ADC was utilized to convert the analogue signal to digital signal, which was then captured by a digital counter. Finally the output of the digital counter was shown on the LCD display to visualize the signal. Besides, a buck converter was utilized to solve the supply voltage mismatch between the ECG signal amplifier (2-3.3 V) and the LCD display (>4.5 V)³⁷. As shown in Supplementary Movie 2, the number on the LCD display increased by 1 every time the heart beats. At the same time, the storage capacitor voltage maintained a positive slope, which showed that the power provided from palm tapping was high enough to power the whole ECG system.

This kind of mechanical power source is also capable of being utilized in various fitness applications. For example, a self-powered pedometer system was realized (Fig. 3d, detailed system diagram shown in Supplementary Fig. 15). In this system, the mechanical sensing part was realized by another attached-electrode TENG. When pressure was applied, this attached-electrode TENG could generate a voltage peak, which made this mechanical sensor consume zero electric power. Similar to the above heart rate signal, this voltage peak signal can be captured by an ADC and a digital counter and then visualized on the LCD display. As shown in Supplementary Movie 3 (Supplementary Movie 7 driven by foot tapping), the number on the LCD display increased by 1 every time pressure was applied on the mechanical sensor. Besides, while the pedometer maintained its normal function, V_{store} increased quickly from the initial value of 5.02 to 5.67 V. This fast increase is from the ultralow system power consumption due to the utilization of the self-powered TENG mechanical sensor.

Besides the self-powered human-activity sensors, this kind of mechanical power unit also has broad applications for other personal electronics. First, its application in wearable electronics is demonstrated through a self-powered wearable watch with mathematical calculation function (Fig. 4a, detailed system diagram shown in Supplementary Fig. 16). As shown in Supplementary Movie 4, a very slow and gentle palm tapping (1 Hz) could drive this wearable watch with full functionality: accurately recording time and calculating square root as an example. Under even irregular palm tapping (have irregular interval between the palming), this wearable watch still remains its normal function (Supplementary Movie 8) as long as the average power provided by human motion is larger than its power consumption. In addition, more complicated data-processing work can also be finished with the power provided by palm tapping. For example, a scientific calculator is a commonly used complicated data-processing system, containing clock generators, registers, read-only memories, arithmetic logic units and a LCD display (Fig. 4b, detailed system diagram shown in



Figure 3 | Application in self-powered human activity sensors. (a) System configuration of self-powered human activity sensors. (b) Demonstration of a self-powered temperature sensor. (c) Demonstration of a self-powered heart rate monitor (ECG) system. (d) Demonstration of a self-powered pedometer.



Figure 4 | Application in self-powered data-processing and transmission system. (a) Demonstration of a self-powered wearable watch and calculator. (b) Demonstration of a self-powered scientific calculator. (c) Demonstration of a self-powered RKE system. (d) Extension of this TENG-based self-charging unit for various applications as a universal adaptable power source.

Supplementary Fig. 17). As shown in Supplementary Movie 5, such an advanced scientific calculator could be easily powered by the mechanical energy from palm tapping. All of the advanced calculation such as trigonometric function, exponent function and logarithm function could be realized without existence of any batteries. Finally, this power unit is applicable in wireless communication system as well. As a typical demo, a remote keyless entry (RKE) module was connected with this power unit and utilized to wirelessly control a car that was about 50 m away. The RKE module is a complicated radio-frequency system, mainly containing a microcontroller and a radio-frequency transmitter (Fig. 4c, detailed system diagram shown in Supplementary Fig. 18). Once the button on the RKE module is pressed, the microcontroller processes and encrypts the signal and transfers the encrypted 64-128-bit data to the radiofrequency transmitter. Then the 433.92 MHz radio-frequency transmitter can send out the code remotely with a data transfer rate about 2-20 kHz. As shown in Supplementary Movie 6, this power unit could charge the storage capacitor from 5.9 to 6.4 V in about 3-5 s. Once the storage capacitor's voltage reached 6.4 V, this RKE unit could functionalize and send out the encrypted signal and the storage capacitor's voltage went back to about 5.9-6.2 V. After receiving this radio-frequency signal, the receiver inside the car could process, decode and respond to this command (unlocking its door and lighting up its low-beam light), clearly showing the success of remote wireless transmission. Then the storage capacitor was charged by this power unit to reach 6.4 V again. From Supplementary Fig. 19, this self-powered wireless remote system has enough power to send out signals to 50 m away in a speed as fast as a command in every 3.06 s.

Discussion

The demos presented above have covered all of the fundamental parts of mobile and wearable systems, including sensors, microcontrollers, memories, arithmetic logic units, displays and even wireless transmitters, which have broad applications in personal sensor systems and internet of things. Besides human biomechanical energy, this kind of designs and concepts can also be extended to other mechanical energy sources, such as rolling wheels, moving cars and trains, blowing wind, and surging waves, by applying various available TENG designs. If high-frequency mechanical agitations are utilized to drastically improve the TENG output power, such system will have a potential to serve as a universal standard power source for sustainably driving more complicated electronic systems, including smart watches, cell phones, navigation system, tablets, personal computers and sensor nodes in internet of things (Fig. 4d).

In summary, we have developed a universal self-charging system driven by random body motion for sustainable operation of mobile and wearable electronics. This power unit can provide a continuous d.c. output as driven by low-frequency $(\sim 2 \text{ Hz})$ human biomechanical energy that could be random in amplitude and frequency, which is enough for sustainable operation of many mobile electronics, such as temperature sensors, heart rate monitoring devices, pedometers, wearable watches, scientific calculators and radio-frequency wireless transmitters. This selfcharging unit is a paradigm shift towards infinite-lifetime energy sources that can never be achieved solely by batteries. The concept proposed in this paper can also be easily extended into other energy harvesters based on piezoelectric and pyroelectric effects. This study overcomes a bottleneck problem towards selfpowered systems, which can have broad applications in mobile/ wearable electronics, internet of things, remote environmental monitor devices and wireless sensor networks.

Methods

Fabrication of nanostructure on FEP surface. A piece of 125-µm FEP film is rinsed with menthol, isopropyl alcohol and deionized water. Then a 10-nm-thick Au is sputtered onto the FEP surface, which will act as the mask for the etching process. Subsequently, this FEP is etched through the inductively coupled plasma (ICP) reactive ion etching for 60 s. The reaction gas is 15.0 sccm Ar, 10.0 sccm O₂ and 30.0 sccm CF₄ in the ICP process. The two ICP power is 400 and 100 W, respectively³⁹.

Fabrication of nanostructure on Al foil. A piece of 50-µm Al foil is pretreated with 0.125 mol1⁻¹ NaOH solution at 40 °C for 1 min. Then the Al foil is rinsed with deionized water, and then used as anode and put into the 80-°C etching solution (3 mol1⁻¹ H₂SO₄ and 1 mol1⁻¹ HCl (3:1)). Graphite electrode plates were utilized as cathode. A constant current density of 150 mA cm⁻² is applied to realize anode oxidation⁴⁰.

Fabrication of multilayered triboelectric nanogenerators. A 125- μ m Kapton film (2.2 inch width) is shaped into a zigzag structure with 10–15 layers. In all, 10–15 layers of aluminium foil and FEP layer are prepared and etched as triboelectric materials. 30 nm Cr/ 300 nm Cu is then e-beam evaporated at the backside of FEP layer. Then these aluminium foils and FEP layers is attached to the substrate. Note that on the front side surface and the backside surface of one layer of Kapton, it must be attached to the same material (Al foil or FEP) to minimize the unnecessary parasitic capacitance that will hurt the performance.

References

- Rogers, J. A. Electronics for the human body. J. Am. Med. Assoc. 313, 561–562 (2015).
- Chortos, A. & Bao, Z. N. Skin-inspired electronic devices. *Mater. Today* 17, 321–331 (2014).
- Wu, H. & Cui, Y. Designing nanostructured Si anodes for high energy lithium ion batteries. *Nano Today* 7, 414–429 (2012).
- Lee, J. et al. Unlocking the potential of cation-disordered oxides for rechargeable lithium batteries. Science 343, 519–522 (2014).
- Goodenough, J. B. & Park, K. S. The Li-ion rechargeable battery: a perspective. J. Am. Chem. Soc. 135, 1167–1176 (2013).
- Paradiso, J. A. & Starner, T. Energy scavenging for mobile and wireless electronics. *IEEE Pervas. Comput.* 4, 18–27 (2005).
- Khaligh, A., Zeng, P. & Zheng, C. Kinetic energy harvesting using piezoelectric and electromagnetic technologies-state of the art. *IEEE Trans. Ind. Electron.* 57, 850–860 (2010).
- Qi, Y. & McAlpine, M. C. Nanotechnology-enabled flexible and biocompatible energy harvesting. *Energy Environ. Sci.* 3, 1275–1285 (2010).
- Yang, Y. et al. Membrane-free battery for harvesting low-grade thermal energy. Nano Lett. 14, 6578–6583 (2014).
- Dresselhaus, M. S. et al. New directions for low-dimensional thermoelectric materials. Adv. Mater. 19, 1043–1053 (2007).
- 11. Steele, B. C. H. & Heinzel, A. Materials for fuel-cell technologies. *Nature* 414, 345–352 (2001).
- Vazquez-Mena, O. *et al.* Performance enhancement of a graphene-zinc phosphide solar cell using the electric field-effect. *Nano Lett.* 14, 4280–4285 (2014).
- Tian, B. Z. et al. Coaxial silicon nanowires as solar cells and nanoelectronic power sources. Nature 449, 885–U888 (2007).
- Beeby, S. P., Tudor, M. J. & White, N. M. Energy harvesting vibration sources for microsystems applications. *Meas. Sci. Technol.* 17, R175–R195 (2006).
- Saha, C. R., O'Donnell, T., Wang, N. & McCloskey, R. Electromagnetic generator for harvesting energy from human motion. *Sens. Actuators A* 147, 248–253 (2008).
- Donelan, J. M. et al. Biomechanical energy harvesting: generating electricity during walking with minimal user effort. Science 319, 807–810 (2008).
- Rome, L. C., Flynn, L., Goldman, E. M. & Yoo, T. D. Generating electricity while walking with loads. *Science* **309**, 1725–1728 (2005).
- 18. Boisseau, S., Despesse, G. & Sylvestre, A. Optimization of an electret-based energy harvester. *Smart Mater. Struct.* **19**, 075015 (2010).
- Lo, H. W. & Tai, Y. C. Parylene-based electret power generators. J. Micromech. Microeng. 18, 104006 (2008).
- Lal, A., Duggirala, R. & Li, H. Pervasive power: a radioisotope-powered piezoelectric generator. *IEEE Pervas. Comput.* 4, 53–61 (2005).
- Boisseau, S., Despesse, G., Ricart, T., Defay, E. & Sylvestre, A. Cantilever-based electret energy harvesters. Smart Mater. Struct. 20, 105013 (2011).
- Perez, M., Boisseau, S., Gasnier, P., Willemin, J. & Reboud, J. L. An electret-based aeroelastic flutter energy harvester. *Smart Mater. Struct.* 24, 035004 (2015).
- 23. Jeon, Y. B., Sood, R., Jeong, J. H. & Kim, S. G. MEMS power generator with transverse mode thin film PZT. *Sens. Actuators A* **122**, 16–22 (2005).

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- McCarty, L. S. & Whitesides, G. M. Electrostatic charging due to separation of ions at interfaces: contact electrification of ionic electrets. *Angew. Chem. Int. Ed.* 47, 2188–2207 (2008).
- 25. Baytekin, H. T. *et al.* The mosaic of surface charge in contact electrification. *Science* **333**, 308–312 (2011).
- Zhu, G., Chen, J., Zhang, T. J., Jing, Q. S. & Wang, Z. L. Radial-arrayed rotary electrification for high performance triboelectric generator. *Nat. Commun.* 5, 3426 (2014).
- Fan, F. R., Tian, Z. Q. & Wang, Z. L. Flexible triboelectric generator. Nano Energy 1, 328–334 (2012).
- Zhang, X. S. *et al.* Frequency-multiplication high-output triboelectric nanogenerator for sustainably powering biomedical microsystems. *Nano Lett.* 13, 1168–1172 (2013).
- Kim, S. et al. Transparent flexible graphene triboelectric nanogenerators. Adv. Mater. 26, 3918–3925 (2014).
- Niu, S. M. & Wang, Z. L. Theoretical systems of triboelectric nanogenerators. Nano Energy 14, 161 (2015).
- Niu, S. M. *et al.* Optimization of triboelectric nanogenerator charging systems for efficient energy harvesting and storage. *IEEE Trans. Electron Devices* 62, 641–647 (2015).
- 32. Wang, S. H. et al. Motion charged battery as sustainable flexible-power-unit. Acs Nano 7, 11263–11271 (2013).
- Niu, S. M. et al. Theoretical study of contact-mode triboelectric nanogenerators as an effective power source. Energy Environ. Sci. 6, 3576–3583 (2013).
- Bai, P. et al. Integrated multi-layered triboelectric nanogenerator for harvesting biomechanical energy from human motions. Acs Nano 7, 3713–3719 (2013).
- Jeong, C. K. et al. Topographically-designed triboelectric nanogenerator via block copolymer self-assembly. Nano Lett. 14, 7031–7038 (2014).
- Nguyen, V. & Yang, R. S. Effect of humidity and pressure on the triboelectric nanogenerator. *Nano Energy* 2, 604–608 (2013).
- Erickson, R. W. & Maksimović, D. Fundamentals of Power Electronics 2nd edn (Kluwer Academic, 2001).
- Boisseau, S., Despesse, G., Monfray, S., Puscasu, O. & Skotnicki, T. Semi-flexible bimetal-based thermal energy harvesters. *Smart Mater. Struct.* 22, 025021 (2013).
- Fang, H., Wu, W. Z., Song, J. H. & Wang, Z. L. Controlled growth of aligned polymer nanowires. J. Phys. Chem. C 113, 16571–16574 (2009).

 Ban, C. L., He, Y. D., Shao, X. & Du, J. Effect of pretreatment on electrochemical etching behavior of Al foil in HCl-H2SO4. *Trans. Nonferrous Met. Soc. China* 23, 1039–1045 (2013).

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Author contributions

S.N. and Z.L.W. conceived the idea; S.N. designed the whole experiment, including the triboelectric nanogenerator and the power management circuit; X.W. and S.N. fabricated the devices; S.N. and X.W. performed all the data measurements; S.N., X.W., F.Y., Y.S.Z. and Z.L.W. discussed all the experimental data; S.N., X.W. and Z.L.W. wrote the manuscript.

Additional information

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